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LAPAROSCOPIC BIPOLAR ELECTROSURGICAL INSTRUMENT**CROSS REFERENCE TO RELATED APPLICATIONS**

This application is a continuation-in-part of U.S. Application Serial No. 09/590,330 filed on June 9, 2000 by Lands et al. entitled "LAPAROSCOPIC BIPOLAR ELECTROSURGICAL INSTRUMENT" which is a continuation of U.S. Application Serial No. 08/970,472 filed on November 14, 1997 by Lands et al. entitled "LAPAROSCOPIC BIPOLAR ELECTROSURGICAL INSTRUMENT", the entire contents of both of these applications are incorporated by reference herein in their entirety.

BACKGROUND*Field of the Invention*

This disclosure relates to an electrosurgical instrument for performing laparoscopic surgical procedures, and more particularly to a laparoscopic electrosurgical instrument that is capable of grasping vessels and vascular tissue with sufficient force between two bipolar jaws to seal the vessel or vascular tissue.

Background of Related Art

Laparoscopic surgical instruments are used to perform surgical operation without making large incisions in the patient. The laparoscopic instruments are inserted into the patient through a cannula, or port, that has been made with a trocar. Typical sizes for cannulas range from three millimeters to twelve millimeters. Smaller cannulas are usually preferred, and this presents a design challenge to instrument manufacturers who must find ways to make surgical instruments that fit through the cannulas.

Certain surgical procedures require cutting blood vessels or vascular tissue. This sometimes presents a problem for surgeons because it is difficult to suture blood vessels using laparoscopic tools. Very small blood vessels, in the range below two millimeters in diameter, can often be closed using standard electrosurgical techniques. If a larger vessel is severed, it may be necessary for the surgeon to convert the laparoscopic procedure into an open-surgical procedure and thereby abandon the benefits of laparoscopy.

Several journal articles have disclosed methods for sealing small blood vessels using electrosurgery. An article entitled Studies on Coagulation and the Development of an Automatic Computerized Bipolar Coagulator, J. Neurosurg., Volume 75, Jul. 1991, describes a bipolar coagulator which is used to seal small blood vessels. The article states that it was not possible to safely coagulate arteries with a diameter larger than 2 to 2.5 mm. A second article is entitled Automatically Controlled Bipolar Electrocoagulation--"COA-COMP", Neurosurg. Rev. (1984), pp. 187-190. This article describes a method for terminating electrosurgical power to the vessel so that charring of the vessel walls can be avoided.

It has been recently determined that electrosurgical methods may be able to seal larger vessels using an appropriate electrosurgical power curve, coupled with an instrument capable of applying a large closure force to the vessel walls. It is thought that the process of coagulating small vessels is fundamentally different than electrosurgical vessel sealing. Coagulation is defined as a process of desiccating tissue wherein the tissue cells are ruptured and dried. Vessel sealing is defined as the process of liquefying the collagen in the tissue so that it cross-links and reforms into a fused mass. Thus, coagulation of small vessels is sufficient to permanently close them. Larger vessels need to be sealed to assure permanent closure.

It would be desirable to have a surgical tool capable of applying electrosurgical energy, capable of applying a large closure force to the vessel walls, and also capable of fitting through a cannula. A large closure force between the jaws typically requires a large moment about the pivot for each

jaw. This presents a challenge because the first and second pins have a small moment arm with respect to the pivot of each jaw. A large force, coupled with a small moment arm, is undesirable because the large forces may shear the first and second pins. It is also undesirable to increase the moment arm of the first and second pins because the physical size of the yoke might not fit through a cannula.

Several bipolar laparoscopic instruments are known. For example, U.S. Pat. No. 3,938,527 discloses a bipolar laparoscopic instrument for tubal cauterization. U.S. Pat. No. 5,250,047 discloses a bipolar laparoscopic instrument with a replaceable electrode tip assembly. U.S. Pat. No. 5,445,638 discloses a bipolar coagulation and cutting forceps with first and second conductors extending from the distal end. U.S. Pat. No. 5,391,166 discloses a bipolar endoscopic instrument having a detachable working end. U.S. Pat. No. 5,342,359 discloses a bipolar coagulation device.

The present invention solves the problem of providing a large closure force between the jaws of a laparoscopic bipolar electrosurgical instrument, using a compact design that fits through a cannula, without risking structural failure of the instrument yoke.

SUMMARY OF THE INVENTION

The present disclosure relates to a laparoscopic bipolar electrosurgical instrument for sealing tissue and includes a handle having an elongated tube affixed thereto. The tube includes first and second jaw members attached to a distal end thereof which are movable from a first position for approximating tissue to at least one subsequent position for grasping tissue therebetween. Each of the jaw members includes an electrically conductive sealing surface. The handle has a fixed handle and a handle which is movable relative to the fixed handle to effect movement of the jaw members from the first position to the at least one subsequent position for grasping tissue. The jaw members are connected to a source of electrosurgical energy such that the jaw members are capable of conducting bipolar electrosurgical energy through the tissue held

therebetween. A stop is included for maintaining a minimum separation distance between opposing sealing surfaces and a ratchet is included for maintaining a closure force in the range of about 3 kg/cm² to about 16 kg/cm² between opposing sealing surfaces. As can be appreciate, the stop member advantageously creates a minimum separation between electrically conductive opposing sealing surfaces to effect an efficient, consistent and uniform tissue seal.

Preferably, the stop maintains a minimum separation distance of at least about 0.03 millimeters between opposing sealing surfaces. Advantageously, the stop maintains a minimum separation distance of about 0.03 millimeters to about 0.16 millimeters. The stop may be disposed on at least one of the electrically conductive sealing surfaces, or alternatively, the stop may be located adjacent one of the electrically conductive sealing surfaces. Although it is preferable to locate the stop member on one or both of the electrically conductive opposing sealing surfaces, it may in some instances be advantageous to locate the stop member adjacent the opposing sealing surfaces.

In one embodiment according to the present disclosure, the first jaw member is connected to the bipolar electrosurgical energy source by a pushrod and the second jaw member is connected to the bipolar electrosurgical source by a conductive tube. As can be appreciated, isolating the jaw members in this manner reduces the likelihood of the instrument short circuiting during activation.

In another embodiment, the ratchet is disposed within the fixed handle and at least one complimentary interlocking mechanical interface is disposed on the movable handle. Preferably, the ratchet and the complimentary interlocking mechanical interface provide at least one interlocking position for maintaining a closure force within the range of about 7 kg/cm² to about 13 kg/cm² between opposing sealing surfaces. Ideally, the closure force is in the range of about 4 kg/cm² to about 6.5 kg/cm². As can be appreciated and as

mentioned herein, maintaining the closure force within the above working ranges is a key factor in producing an effective and consistent seal.

In yet another embodiment according to the present disclosure, the laparoscopic bipolar electrosurgical instrument includes a handle having an elongated tube affixed thereto with first and second jaw members attached to a distal end thereof which each include electrically conductive sealing surfaces. The jaw members are movable from a first position for approximating tissue to at least one subsequent position for grasping tissue therebetween. The handle has a fixed handle and a handle which is movable relative to the fixed handle to effect movement of the jaw members from the first position to at least one subsequent position for grasping tissue. Advantageously, the sealing surfaces include a non-stick material for reducing tissue adhesion during the sealing process. The first and second jaw members are coupled to a source of bipolar electrosurgical energy and a stop is disposed on at least one of the electrically conductive sealing surfaces to maintain a minimum separation distance between the opposable seal surfaces during sealing.

A ratchet is disposed on one of the fixed and movable handles and at least one complimentary interlocking mechanical interface is disposed on the other of the fixed and movable handles. Advantageously, the ratchet and the complimentary interlocking mechanical interface include at least one interlocking position which maintains a closure force in the range of about 7 kg/cm² to about 13 kg/cm² between opposable seal surfaces.

In one embodiment, the non-stick material is a coating which is deposited on the opposable sealing surfaces. As can be appreciated, this reduces the likelihood of coagulum build-up and sticking. The non-stick coating may be selected from a group of materials consisting of: nitrides and nickel/chrome alloys. Preferably, the non-stick coating includes one of: TiN; ZrN; TiAlN; CrN; nickel/chrome alloys with a Ni/Cr ratio of approximately 5:1; Inconel 600; Ni200; and Ni201.

In one embodiment according to the present disclosure, the opposable sealing surfaces are manufactured from a non-stick material which is a nickel/chrome alloy. For example, the non-stick material may include nickel/chrome alloys with a Ni/Cr ratio of approximately 5:1, Inconel 600, Ni200 and Ni201. It is envisioned that these particular materials are advantageous in providing a superior non-stick surface which reduces coagulum build-up and sticking during activation.

Preferably, at least one of the jaw members, handles and elongated tube includes an insulative material disposed thereon which may advantageously be an insulative coating or an insulative sheath.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a perspective view of a laparoscopic bipolar electrosurgical instrument according to the present disclosure;

FIG. 2 is a perspective view of the distal end and jaws of the instrument in FIG. 1;

FIG. 3 is an exploded view of the distal end shown in FIG. 2;

FIG. 4 is perspective view of the distal end of the instrument with the jaws removed;

FIG. 5 is another perspective of FIG. 4;

FIG. 6 is a side view of an electrical spring contact; and

FIG. 7 is a front view of the spring contact shown in FIG. 6.

DETAILED DESCRIPTION OF THE INVENTION

A laparoscopic bipolar electrosurgical instrument 10 is shown in FIG. 1. The instrument 10 has a proximal end 11 with a handle 14 for holding and manipulating the instrument 10. A distal end 12 on the instrument 10 is used for surgical manipulation of tissue. The instrument 10 comprises an elongate tube 13 that is sized to fit through a cannula for laparoscopic operations, and in different embodiments may be sized to fit through a five to ten millimeter cannulas.

A portion of the distal end 12 of the instrument 10 is shown in FIG. 2. A first jaw 15 and a second jaw 16 are shown in an open position. An angle α is subtended by the jaws 15 and 16. Closing of the jaws 15 and 16 is defined as a reduction of the angle α subtended by the jaws 15 and 16. Similarly, opening of the jaw 15 and 16 is defined as an enlargement of the angle α . The angle α is zero when the jaws 15 and 16 are closed together. The center of rotation for the first jaws 15 is at the first pivot 41, and the center of rotation for the second jaw 16 is at the second pivot 42. The first pivot 41 is located on an outer nose piece 32, and fits in a first pivot hole 43 located on the first flange 18. The second pivot 42 is located on an inner nose piece 31, and fits in a second pivot hole 44 located on the second flange 20.

Pieces that comprise the distal end 12 of the instrument 10 are shown in an exploded view in FIG. 3. The first jaw 15 and the second jaw 16 are shown separated from a yoke 17. The first jaw 15 has a first flange 18 and a first slot 19 therewithin. The second jaw 16 has a second flange 20 and a second slot 21 therewithin. Each jaw 15 and 16 is preferably formed from a single piece of stainless steel or other electrically conductive material.

Referring again to FIG. 3, the yoke 17 is attached to a pushrod 22. The yoke 17 is preferably formed from an electrically insulative material such as plastic. A first side 23 of the yoke 17 faces the first flange 18. A second side 24 of the yoke 17 faces the second flange 20. When the yoke 17 is positioned between the flanges 18 and 20, the yoke 17 also acts to electrically insulate the

first jaw 15 from the second jaw 16. In this manner, bipolar electrosurgical current can be conducted through tissue grasped by the jaws 15 and 16 without short circuiting between the flanges 18 and 20.

A first pin 25 is located on the first side 23 which movably engages the first slot 19. Similarly, a second pin 26 is located on the second side 24 to movably engage the second slot 21. Each pin and slot combination works as a cam-follower mechanical linkage. Motion of the pushrod 22 moves the yoke 17 causing pins 25 and 26 to slide within their respective slots 19 and 21. The slots 19 and 21 are angled with respect to the distal ends of the jaws 15 and 16 such that the jaws 15 and 16 move in an arcuate fashion toward and away from each other. The pins 25 and 26 are different from the pivots 41 and 42. The pins 25 and 26 provide a force against the walls of the slots 19 and 21, creating a moment about the pivots 41 and 42.

The slots 19 and 21 are arranged such that distal motion of the pushrod 22 causes the jaws 15 and 16 to move together. Distal motion of the pushrod 22 is defined as motion in the direction of the distal end 12 of the instrument 10. Once the jaws 15 and 16 are closed together, the present invention holds the jaws 15 and 16 together with a compressive force on the pushrod 22.

One of the advantages of this invention is that shear forces on the pins 25 and 26 can be offloaded to prevent mechanical failure when large forces are being transmitted to the jaws 15 and 16. Each slot 19 and 20 has a cul-de-sac 27 and 28, respectively, as shown in FIG. 3. The first cul-de-sac 27 is an enlargement of the first slot 19 near its distal end. The second cul-de-sac 28 is an enlargement of the second slot 21 near its distal end. The cam-follower motion of the pins 25 and 26 in the slots 19 and 21 will bring the pins 25 and 26 into their respective cul-de-sac 27 and 28. This position of the pins 25 and 26 leaves a very small moment arm between the pins 25 and 26 and the pivots 41 and 42. The yoke 17 has shoulders 29 and 30 that can provide a relatively large moment about the pivots 41 and 42 to effect a high closure force between the jaws 15 and 16 without a high shear forces on the pins 25 and 26, as described below.

Once the pins 25 and 26 are in the cul-de-sacs 27 and 28, the force from the yoke is transmitted to the flanges 18 and 20 by a first shoulder 29 and a second shoulder 30. The shoulders 29 and 30 abut the proximal end of the flanges 18 and 20 to cause the jaws 15 and 16 to close together. The pivots 41 and 42 are preferably made of metal and can withstand relatively high shear forces. In contrast, pins 25 and 26 are preferably made of plastic and will break under relatively high shear forces. Thus, the shoulders 29 and 30 provide a moment about the pivots 41 and 42, thereby avoiding the necessity of applying high shear forces to the pins 25 and 26 wherein the moment arm from the pins 25 and 26 would be small. There is an angle α at which the pins 25 and 26 enter their respective cul-de-sacs 27 and 28 and the shoulders 29 and 30 abut the flanges 18 and 20. The angle α at which the forgoing occurs is preferably around three degrees.

The bipolar electrosurgical instrument 10 has first and second poles of alternating potential that are conducted along the instrument 10 and through tissue that is grasped between the jaws 15 and 16. The first pole is conducted from the proximal end 11 toward the distal end 12 along the pushrod 22. The second pole is conducted from the proximal end 11 toward the distal end 12 along the tube 13. The outer surface of the tube 13 is preferably coated with an electrically insulative material. There is also preferably an electrically insulative barrier between the pushrod 22 and the tube 13 to prevent short circuits in the instrument 10.

In the preferred embodiment, the distal end of the instrument 10 comprises an inner nose piece 31 and an outer nose piece 32, as shown in FIG. 2. The inner nose piece 31 is electrically connected with the pushrod 22, while the outer nose piece is electrically connected with the tube 13. The inner nose piece 31 and the outer nose piece 32 capture the yoke 17, along with the first and second flanges 18 and 20, as shown in FIG. 2. The yoke 17 moves axially, along an axis defined by the tube 13, in a space between the inner and outer nose pieces 31 and 32. A spacer stake 33 maintains the separation of the nose pieces 31 and 32 at their distal ends. The nose pieces 31 and 32 provide

lateral support for the flanges 18 and 20 to help ensure that the pins 25 and 26 remain within the slots 19 and 21, respectively.

The preferred embodiment also comprises an inner insulator 34 and an outer insulator 35 for maintaining electrical insulation between the poles. The outer insulator 35 is seated between the tube 13 and the inner nose 31, as shown in FIGS. 2 and 4. The inner insulator 34 is seated between the tube 13 and the pushrod 22. In this manner, the outer nose piece 32 can provide electrical continuity between the tube 13 and the second jaw 16, while the inner nose piece 34 can provide electrical continuity between the pushrod 22 and the first jaw 15. Since the pushrod 22 is slidably mounted within the tube 13, the preferred embodiment has a spring contact 36, as shown in FIGS. 6 and 7, which is mounted on the pushrod 22 to maintain an electrical connection with the inner nose piece 34 during axial motion.

The first and second jaws 15 and 16 each have ridges 37 and 38 at their distal ends that preferably nest together. The jaws 15 and 16 also have seal surfaces 39 and 40, as shown in FIG. 2. The width of the seal surfaces 39 and 40 is a parameter that affects the quality of the surgical outcome. The closure force between the jaws 15 and 16 varies along the length of the seal surfaces 39 and 40, with the largest force at the distal tip and the smallest force at the proximal end of the seal surfaces 39 and 40. It is known that the amount of pressure exerted on the tissue depends on the surface area of the tissue that is in contact with the seal surfaces. In the one embodiment, the width of each seal surface, e.g., 39, is in the range of about 2 to about 5 millimeters, and preferably 4 millimeters width, while the length of each seal surface 39 and 40 is preferably in the range of about 10 to 30 millimeters.

It has been found through experimentation that good vessel sealing results are obtained when the closure force in grams divided by the width in millimeters is in the range of about 400 to 650 grams per millimeter of seal surface width. Since the closure force varies with the length of the seal surfaces 39 and 40, it has been found to be advantageous to taper the width of the seal surfaces 39 and 40 along their length, with the widest width at the

proximal end and the narrowest width at the distal end. For example, if the width of the seal surface 39, 40 is 4 millimeters, the closure force is preferably in the range of about 1600 grams to about 2600 grams. This design allows the jaws 15 and 16 to apply a relatively constant closure force per unit width, preferably 525 grams per millimeter width which yields a closure force of 2100 grams for a 4 millimeter width seal surface 39, 40.

In one embodiment, the handle 14 includes a fixed handle 50 having a channel 51 defined therein which slidably receives a movable handle 52. Movable handle 52 includes a handgrip 53 defined therein which allows a user to move handle 52 relative to fixed handle 50. Movable handle 52 also includes a flange 55 having a series of grooves 62 defined therein which mechanically inter-engage a corresponding ratchet 60 disposed within channel 51. Preferably, the ratchet 60 and groove 62 are dimensioned such that successive ratchet positions will yield pressures within a predetermined working range of about 7 kg/cm² to about 13 kg/cm². In one embodiment, the successive ratchet positions are two millimeters apart.

Experimental results in tissue studies suggest that the magnitude of pressure exerted on the tissue by the seal surfaces 39 and 40 is important in assuring a proper surgical outcome. Tissue pressures within a working range of about 3 kg/cm² to about 16 kg/cm² and, preferably, within a working range of 7 kg/cm² to 13 kg/cm² have been shown to be effective for sealing arteries and vascular bundles. Tissue pressures within the range of about 4 kg/cm² to about 6.5 kg/cm² have proven to be particularly effective in sealing arteries and tissue bundles.

A method of making a laparoscopic bipolar electrosurgical instrument 10 is also herein described. The method comprises the step of forming a first jaw 15 having a first flange 18 with a first slot 19, and a second jaw 16 having a second flange 20 with a second slot 21. The jaws 15 and 16 are preferably formed in a casting process, although it is also possible to machine the jaws 15 and 16 from stock. The casting process may include injecting powdered metal under pressure into a mold, and then applying heat.

Other steps in the method include attaching a yoke 17 to a pushrod 22, and electrically insulating the first flange 18 from the second flange 20 with the yoke 17. The yoke 17 is preferably an injection molded plastic part with features including a first shoulder 29 and a second shoulder 30.

During assembly of the distal portion of the instrument 10, steps in the method include engaging a first pin 25 with the first slot 19, and engaging a second pin 26 with the second slot 21. The slots 19 and 21 are shaped such that a subtended angle α between the first and second jaws 15 and 16 decreases with distal motion of the pushrod 17. The slots 19 and 20 are formed with cul-de-sacs 27 and 28 positioned to relieve shear stresses on the first and second pins 25 and 26 at the subtended angle α approximately where the first and second shoulders 29 and 30 engage the first and second flanges 18 and 20.

Further steps in the method comprise: surrounding at least a portion of the pushrod 22 with an electrically conductive tube 13; electrically insulating the tube 13 from the pushrod 22; electrically connecting an inner nose piece 31 to the pushrod 22, and electrically connecting an outer nose piece 32 to the tube 13, wherein the inner nose piece 31 and the outer nose piece 32 capture the yoke 17 along with the first and second flanges 18 and 20 to conduct bipolar electrosurgical current to the first and second jaws 15 and 16. In the preferred embodiment, there is a step of electrically connecting the pushrod 22 and the inner nose piece 31 with a spring contact 36.

The method of making the instrument 10, in some embodiments, includes the steps of tapering the width of the seal surfaces 39 and 40 along the length of each of the first and second jaws 15 and 16.

An electrically insulative coating 70 may be included to substantially cover the elongated tube 13 to protect the surgeon against electrical arcs. Other parts of the instrument may also be protected by the insulative coating 70. An insulative sheath may also be used to cover tube 13 or other

components of the instrument 10, e.g., the proximal end 11, handles 50, 52 and the outer surfaces (non-opposing surfaces) of the jaw members 15, 16.

It is envisioned that the outer surface of the jaw members 15 and 16 may include a nickel-based material, coating, stamping, metal injection molding which is designed to reduce adhesion between the jaw members (or components thereof) with the surrounding tissue during activation and sealing. Moreover, it is also contemplated that other components such as the tube 13 and handles 50, 52 may also be coated with the same or a different "non-stick" material. Preferably, the non-stick materials are of a class of materials that provide a smooth surface to prevent mechanical tooth adhesions.

It is also contemplated that the tissue sealing surfaces 39 and 40 of the jaw members 15 and 16, respectively, may be manufactured from one (or a combination of one or more) of the following "non-stick" materials: nickel-chrome, chromium nitride, MedCoat 2000 manufactured by The ElectroLizing Corporation of OHIO, Inconel 600 and tin-nickel. For example, high nickel chrome alloys and Ni200, Ni201 (~100% Ni) may be made into electrodes or sealing surfaces by metal injection molding, stamping, machining or any like process.

In addition these materials preferably include an optimal surface energy for eliminating sticking due in part to surface texture and susceptibility to surface breakdown due electrical effects and corrosion in the presence of biologic tissues. It is envisioned that these materials exhibit superior non-stick qualities over stainless steel and should be utilized on the instrument in areas where the exposure to pressure and RF energy can create localized "hot spots" more susceptible to tissue adhesion. As can be appreciated, reducing the amount that the tissue "sticks" during sealing improves the overall efficacy of the instrument.

The tissue sealing surfaces 39 and 40 may also be "coated" with one or more of the above materials to achieve the same result, i.e., a "non-stick surface". For example, Nitride coatings (or one or more of the other above-

identified materials) may be deposited as a coating on another base material (metal or nonmetal) using a vapor deposition manufacturing technique.

One particular class of materials disclosed herein has demonstrated superior non-stick properties and, in some instances, superior seal quality. For example, nitride coatings which include, but are not limited to: TiN, ZrN, TiAlN, and CrN are preferred materials used for non-stick purposes. CrN has been found to be particularly useful for non-stick purposes due to its overall surface properties and performance. Other classes of materials have also been found to reducing overall sticking. For example, high nickel/chrome alloys with a Ni/Cr ratio of approximately 5:1 have been found to significantly reduce sticking in bipolar instrumentation. One particularly useful non-stick material in this class is Inconel 600. Bipolar instrumentation having electrodes made from or coated with Ni200, Ni201 (~100% Ni) also showed improved non-stick performance over typical bipolar stainless steel electrodes.

It has been found experimentally that local current concentrations can result in an uneven tissue effect, and to reduce the possibility of this outcome, each seal surface 39 and 40 may include a radiused edge 80, 81. As mentioned above, a tapered seal surface 39 and 40 has been shown to be advantageous in certain embodiments because the taper allows for a relatively constant pressure on the tissue along the length of the seal surfaces 39 and 40. The width of the seal surfaces 39 and 40 may be adjusted to assure that the closure force divided by the width is approximately constant along the length.

In one embodiment, a stop 90, made from insulative material, is located in the instrument to maintain a minimum separation of at least about 0.03 millimeters between the seal surfaces 39 and 40, as shown in FIG. 3. Preferably, the stop maintains a minimum separation distance in the range of about 0.03 millimeters to about 0.16 millimeters. The stop 90 reduces the possibility of short circuits between the seal surfaces 39 and 40. It is envisioned that stop 90 may be positioned proximate the pivots 41 and 42, proximate the stake 33 or adjacent the opposable seal surfaces 39 and 40.

In another embodiment, the instrument 10 includes a second or alternative stop 95 which is designed to maintain a minimum separation of at least about 0.03 millimeters between the seal surfaces 39 and 40, as shown in FIG. 2. Preferably, the stop 90 and/or the stop 95 maintains a separation distance within the range of about 0.03 millimeters to about 0.16 millimeters. A plurality of stops 90 and/or 95 (or various patterns of stops 90, 95) may also be utilized to accomplish this purpose.

It is to be understood that the above described embodiments are only illustrative of the application of the principles of the present invention. Numerous modifications and alternative arrangements may be devised by those skilled in the art without departing from the spirit and scope of the present invention. The appended claims are intended to cover such modifications and arrangements.